BACKGROUND: CPAP improves respiratory function in prematurely born infants by establishing and maintaining functional residual capacity, but the level of CPAP that optimizes respiratory function has not been adequately described. We compared ventilation efficiency and respiratory muscle function at different levels of CPAP.

METHODS: We studied spontaneously breathing, intubated convalescent premature infants at King’s College Hospital NHS Foundation Trust and calculated the ventilation efficiency index and the respiratory muscle time constant of relaxation ($r$) at the end of 3 consecutive 5-min periods at 4, 6, and 8 cm H$_2$O of CPAP delivered in random order.

RESULTS: Between February 2016 and August 2016, 38 infants with a median gestational age of 27 (interquartile range [IQR], 25–30) weeks and a median birthweight of 0.88 (IQR, 0.73–1.02) kg were studied. At a CPAP level of 6 cm H$_2$O, the median ventilation efficiency index was higher (1.52 [IQR, 1.02–2.27]) and median $r$ was lower (15.6 [IQR, 10.1–21.3]) s/cm H$_2$O compared with the median ventilation efficiency index (0.75 [IQR, 0.56–1.03]) and median $r$ (23.3 [IQR, 15.4–35.2] sec/cm H$_2$O) at CPAP of 4 cm H$_2$O ($P < .001$ for both). At a CPAP level of 8 cm H$_2$O, median ventilation efficiency index was significantly lower (1.27 [IQR, 1.04–1.91]) and median $r$ was not significantly different (11.2 [IQR, 8.3–18.9] s/cm H$_2$O) compared with ventilation efficiency index and $r$ at CPAP of 6 cm H$_2$O ($P < .001$ and $P = .12$, respectively). After multiple logistic regression, the level of CPAP was independently associated with the ventilation efficiency index (adjusted $P < .001$) and $r$ (adjusted $P = .003$).

CONCLUSIONS: Increasing the level of CPAP from 4 to 6 cm H$_2$O was associated with enhanced ventilation efficiency and respiratory muscle function in convalescent premature infants on ventilation, but there was no further benefit from increasing the pressure $>6$ cm H$_2$O. Key words: continuous positive airway pressure; ventilation efficiency; respiratory muscle function; respiratory muscle rate of relaxation; newborn infants; premature.

Introduction

CPAP is widely used in neonatal intensive care as a form of noninvasive respiratory support. CPAP improves respiratory function in prematurely born infants by increasing the functional residual capacity and splinting open the upper airway. Although numerous studies have qualitatively described the beneficial effect of CPAP on respiratory function, few studies have investigated the optimal value of the distending pressure. Theoretically, a very low distending pressure would allow for atelectasis, which negatively impacts on oxygenation and increases the work of breathing by imposing the added work of...
opening atelectatic areas breath by breath. However, this version may differ from the final published version in the online and print editions of RESPIRATORY CARE

Few studies have investigated the effect of increasing levels of CPAP on respiratory function. Those studies were conducted in populations that consisted of 10 to 20 infants who received noninvasive CPAP by using electrical impedance tomography, respiratory, or electromagnetic inductive plethysmography. Results of these studies concluded that increasing levels of CPAP increased the expiratory lung volume and decreased the work of breathing. To our knowledge, there is no published evidence on the effect of varying levels of CPAP on composite indices of ventilation efficiency or respiratory muscle function in prematurely born infants. Yet, such a relationship would be plausible because adult studies demonstrate an unloading of the respiratory muscles with the application of CPAP and infants with bronchiolitis also manifest improved inspiratory muscle efficiency and respiratory muscle unloading when treated with CPAP. The aim of this study was to compare ventilation efficiency and respiratory muscle function at 3 different CPAP levels (4, 6, and 8 cm H2O) that are currently used in clinical practice.

Methods

Subjects

We retrospectively analyzed data collected during a study that assessed readiness for extubation. At King’s College Hospital NHS Foundation Trust, infants born at <34 completed weeks of gestation without congenital anomalies and were on ventilation were eligible for study. The infants were ventilated with a Cole’s endotracheal tube (size 2.5 or 3.0 mm) on volume-targeted or pressure-controlled time-cycled ventilation with the SLE5000 neonatal ventilator or the SLE2000 infant ventilator (SLE, Croydon, United Kingdom). The study was approved by the London–Surrey Borders Research Ethics Committee. Written, informed parental consent was obtained. The study was registered with the Health Research Authority, NHS England (IRAS ID 193377).

Study Protocol

The infants were studied when they were clinically stable and ready for extubation. Extubation was considered, according to the unit policy, when FiO2 was < 0.4, the infant had a pH of >7.25, Pco2 of <65 mm Hg, and the breathing frequency was higher than the set ventilator rate. All infants < 34 weeks of postmenstrual age were receiving caffeine, and sedation was discontinued at least 12 h before measurement. When the clinical team decided that an infant was ready for extubation, the infant was switched from mechanical ventilation to endotracheal CPAP, and flow, volume, airway pressure, and expired CO2 were recorded. Each infant spent a total of 15 min on endotracheal CPAP, which consisted of 3 separate periods at CPAP levels of 4, 6, and 8 cm H2O delivered in random order. During the spontaneous breathing on endotracheal CPAP, the oxygen saturation and heart rate were monitored.

Measuring Equipment

The NM3 respiratory profile monitor (Philips Respironics, Wallingford, Connecticut) was used to measure flow, volume, airway pressure, and the concentration of expired CO2. The monitor was connected to a laptop (Dell Latitude, Dell, Bracknell, United Kingdom) with customized Spectra software 3.0.1.6, 2016 (Grove Medical, London, United Kingdom). The NM3 respiratory profile monitor had a combined CO2 and flow sensor that was placed between the endotracheal tube and the ventilator circuit.
Expired CO₂ was measured with a Capnostat-5 mainstream, infrared absorption spectroscopy CO₂ sensor with a dead space of <1 mL (Philips Respironics).

**Calculation of the Ventilation Efficiency Index and the Respiratory Muscle Time Constant or Relaxation**

The ventilation efficiency index was calculated from the formula:

\[
\text{Ventilation efficiency index} = \frac{3,800}{\Delta P} \times f \times P_{\text{ETCO}_2}
\]

Where 3,800 is a constant for production of CO₂ (mL/mm Hg kg/min), \(\Delta P\) is the difference between the spontaneously generated inspiratory pressure and the level of CPAP in mm Hg, \(f\) is the breathing frequency during spontaneous breathing, and \(P_{\text{ETCO}_2}\) is the end-tidal carbon dioxide pressure in mm Hg. The respiratory muscle time constant of relaxation (\(\tau\)) is an index of respiratory muscle fatigue and is calculated as the reciprocal of the absolute value of the slope of the pressure decline as a function of time at the lower 60% of the curve (Fig. 1). Higher values of \(\tau\) signify a slower relaxation and impaired respiratory muscle function, whereas lower values of \(\tau\) signify a faster relaxation and more efficient respiratory muscle function. The part of the airway pressure trace with smooth decay was hand selected and analyzed. Breaths with a waveform that exhibited evidence of expiratory diaphragmatic braking were excluded from the analysis. For each subject, the mean \(\tau\) value of at least 5 consistent breaths was recorded. All assessments of airway pressure, \(f\), and \(P_{\text{ETCO}_2}\) were undertaken at the last minute of the 5-min period spent at each level of CPAP. For the calculation of the ventilation efficiency index, the mean of all values of airway pressure and \(P_{\text{ETCO}_2}\) during the last minute of the 5-min period were analyzed.

**Information From the Medical Records**

Sex, gestational age, birthweight, postmenstrual age, postnatal age, weight at the time of measurement, and total days of ventilation before the study were recorded. Birthweight z scores were calculated based on British national reference data. The \(F_{\text{IO}_2}\) and the \(P_{\text{aCO}_2}\) within 30 min before the measurement were also recorded from the nursing observation charts. Information recorded from the infant’s medical notes included whether the infant had a patent ductus arteriosus, had been exposed to antenatal steroids, were given postnatal surfactant, or had had an intraventricular hemorrhage. A patent ductus arteriosus was diagnosed clinically and confirmed by echocardiography. Administration of antenatal corticosteroids was recorded as positive if at least 2 doses were given. The cranial ultrasound was recorded as normal if there was no intraventricular hemorrhage or intracranial pathology.

**Sample Size**

We retrospectively justified the size of our sample as sufficient to detect clinically important differences in the ventilation efficiency index. Pillow et al reported improved ventilation efficiency in an animal model of premature lambs at a mean (SD) difference in ventilation efficiency index of 0.10 (0.08). Based on the above, 14 subjects would enable detection of a difference in ventilation efficiency index of 0.10 at different levels of CPAP, with 90% power at the 5% level.

**Statistics**

Data were tested for normality with the Kolmogorov–Smirnoff test and were found to be non-normally distributed. Hence, differences in tidal volume (\(V_T\), \(f\), inspiratory pressure, \(P_{\text{ETCO}_2}\), ventilation efficiency index, and \(\tau\) at different CPAP levels were assessed for statistical significance by using the Kruskal-Wallis rank-sum test. The 2-tailed Mann-Whitney U test was used for pairwise post hoc comparisons between the individual groups. To assess the adjusted effect of the different levels of CPAP on the pulmonary function indices, the factors that were significantly different between the groups according to the level of CPAP (\(P < .05\)) were inserted into a multiple logistic regression model with the level of CPAP as the outcome variable. Variables without normal distribution were logarithmically transformed. Multi-collinearity among the independent variables in the regression analysis was assessed by calculation of the tolerance for the inde-
VENTILATION EFFICIENCY AND RESPIRATORY MUSCLE FUNCTION IN PREMATURE INFANTS

Table 1. Demographics and Ventilator Settings of the Included Infants

<table>
<thead>
<tr>
<th>Parameter</th>
<th>Result</th>
</tr>
</thead>
<tbody>
<tr>
<td>Gestational age, median (IQR) wk</td>
<td>26.6 (25.0–29.5)</td>
</tr>
<tr>
<td>Birth weight, median (IQR) kg</td>
<td>0.88 (0.73–1.02)</td>
</tr>
<tr>
<td>Birth weight z score, median (IQR)</td>
<td>−0.56 (−1.59 to 0.10)</td>
</tr>
<tr>
<td>Boys, n (%)</td>
<td>19 (50)</td>
</tr>
<tr>
<td>Age at study, median (IQR) d</td>
<td>11 (4–43)</td>
</tr>
<tr>
<td>PMA at study, median (IQR) wk</td>
<td>30.6 (27.5–33.5)</td>
</tr>
<tr>
<td>PDA, n (%)</td>
<td>8 (21)</td>
</tr>
<tr>
<td>Antenatal steroids, n (%)</td>
<td>31 (82)</td>
</tr>
<tr>
<td>Postnatal surfactant, n (%)</td>
<td>38 (100)</td>
</tr>
<tr>
<td>Caffeine at study, n (%)</td>
<td>38 (100)</td>
</tr>
<tr>
<td>IVH grade II, III, or IV, n (%)</td>
<td>9 (24)</td>
</tr>
<tr>
<td>FIO2, median (IQR)</td>
<td>0.27 (0.22–0.36)</td>
</tr>
<tr>
<td>Mean airway pressure, median (IQR) cm H2O</td>
<td>8 (7–9)</td>
</tr>
<tr>
<td>PECO2, median (IQR) mm Hg</td>
<td>47.7 (41.2–53.0)</td>
</tr>
<tr>
<td>pH, median (IQR)</td>
<td>7.36 (7.32–7.41)</td>
</tr>
<tr>
<td>Ventilation days before the study, median (IQR)</td>
<td>8 (3–35)</td>
</tr>
</tbody>
</table>

N = 38.
IQR = interquartile range
PMA = postmenstrual age
PDA = patent ductus arteriosus
IVH = intraventricular hemorrhage

Results

Between February 1, 2016, and August 1, 2016, 38 infants (19 boys) with a median gestational age of 26.6 (IQR, 25.0–29.5) wk and a median birthweight of 0.88 (IQR, 0.73–1.02) kg were included in the study (Table 1). All the infants were given surfactant after birth. The infants were studied at a median postmenstrual age of 30.6 (IQR, 27.5–33.5) wk and at the time of the study had a median FIO2 requirement of 0.27 (IQR, 0.22–0.36), and median PECO2 of 47.7 (IQR, 41.2–53.0) mm Hg (Table 1). The VT/kg of body weight and the PETCO2 levels were not significantly different at CPAP levels of 4, 6, or 8 cm H2O (Table 2).

CPAP of 4 Versus 6 cm H2O

At a CPAP level of 6 cmH2O, the median inspiratory pressure and ventilation efficiency index were significantly higher compared with the inspiratory pressure and ventilation efficiency index, at a CPAP level of 4 cm H2O (P < .001 for both) (Table 2, Fig. 2). At a CPAP level of 6 cm H2O, the median τ was lower compared with the τ at a CPAP level of 4 cm H2O (P = .005) (Table 2).

CPAP of 6 Versus 8 cm H2O

At a CPAP level of 8 cm H2O, the median inspiratory pressure was higher compared with the inspiratory pressure at a CPAP level of 6 cm H2O. At a CPAP level of 8 cm H2O, the median ventilation efficiency index was lower compared with the ventilation efficiency index at a CPAP level of 6 cm H2O (P < .001) (Table 2, Fig. 2). At a CPAP level of 8 cm H2O, the median τ was not significantly lower compared with the τ at a CPAP level of 6 cm H2O (P = .12) (Table 2). Multivariate regression analysis demonstrated that the level of CPAP was independently associated with inspiratory pressure (adjusted P < .001), ventilation efficiency index (adjusted P < .001), and τ (adjusted P = .003) but not with f (Table 3).

Discussion

We demonstrated that increasing the distending pressure on CPAP from 4 to 6 cm H2O was associated with an improvement in ventilation efficiency and respiratory muscle function, but a further increase to 8 cm H2O was associated with decreased ventilation efficiency and no further improvement in respiratory muscle function. Previous studies report how increasing the level of CPAP affects respiratory function.6-8,18 Elgellab et al7 used respiratory inductive plethysmography to measure lung volumes in 10 premature infants on nasal CPAP at a pressure of 0, 2, 4, 6, and 8 cm H2O, and reported that increased pressure was associated with a higher end-expiratory lung volume, higher VT, and less thoraco-abdominal asynchrony. More recently, Miedema et al6 used electrical impedance tomography in 22 premature infants at a pressure of 2, 4, and 6 cm H2O, and similarly reported an increase in end-expiratory lung volume and VT, and a decrease in thoraco-abdominal asynchrony with increased CPAP. Pickerd et al8 used electromagnetic inductive plethysmography at 5, 7, and 9 cm H2O, and reported higher VT with higher CPAP levels.

Furthermore, Bhatia et al18 studied 20 premature infants with electrical impedance tomography and demonstrated that manipulation of the distending pressure can be used as a maneuver to optimize lung volume in the preterm lung. Our study complemented the literature by studying a larger cohort, which consisted of extremely premature infants at a critical time before extubation when the level of postextubation support would be decided. Furthermore, our study reported that the beneficial effects of CPAP on ventilation efficiency and respiratory muscle function did not persist beyond the level of 6 cm H2O, because, at a level of 8 cm H2O, ventilation efficiency was significantly re-
Ventilation efficiency and respiratory muscle function in premature infants

Table 2. Pulmonary Function Assessments According to Level of CPAP Data

<table>
<thead>
<tr>
<th>Variable</th>
<th>4 cm H₂O</th>
<th>6 cm H₂O</th>
<th>8 cm H₂O</th>
<th>P</th>
</tr>
</thead>
<tbody>
<tr>
<td>Vₜ, mL</td>
<td>7.2 (5.3–9.7)</td>
<td>7.3 (5.7–9.0)</td>
<td>7.8 (6.3–9.6)</td>
<td>.78</td>
</tr>
<tr>
<td>Vₜ, mL/kg</td>
<td>5.7 (4.6–6.8)</td>
<td>6.1 (5.3–7.4)</td>
<td>6.6 (5.8–7.6)</td>
<td>.10</td>
</tr>
<tr>
<td>f</td>
<td>73 (63–84)</td>
<td>67 (59–76)</td>
<td>60 (50–73)</td>
<td>.007*</td>
</tr>
<tr>
<td>Spontaneously generated inspiratory pressure, cm H₂O</td>
<td>5.7 (5.4–6.7)</td>
<td>7.1 (6.4–7.6)</td>
<td>9.2 (8.8–9.8)</td>
<td>&lt;.001†</td>
</tr>
<tr>
<td>Pspell, mm Hg</td>
<td>45.3 (36.1–52.0)</td>
<td>41.9 (35.1–47.3)</td>
<td>40.4 (35.3–45.6)</td>
<td>.48</td>
</tr>
<tr>
<td>Ventilation efficiency index</td>
<td>0.75 (0.56–1.03)</td>
<td>1.52 (1.02–2.27)</td>
<td>1.27 (1.04–1.91)</td>
<td>&lt;.001‡</td>
</tr>
<tr>
<td>τ, s/cm H₂O</td>
<td>23.3 (15.4–35.2)</td>
<td>15.6 (10.1–21.3)</td>
<td>11.2 (8.3–18.9)</td>
<td>.001§</td>
</tr>
</tbody>
</table>

Data are median (interquartile range).
*For post hoc tests: P = .002 only for 4 vs 8 and 4 vs 6 cm H₂O; nonsignificant for 6 vs 8 cm H₂O.
†For post hoc tests: P < .001 for 4 vs 6, 6 vs 8, and 4 vs 8 cm H₂O.
‡For post hoc tests: P = .005 for 4 vs 6 cm H₂O, P < .001 for 4 vs 8 cm H₂O, and nonsignificant for 6 vs 8 cm H₂O.
§For post hoc tests: P = .005 for 4 vs 6 cm H₂O, P < .001 for 4 vs 8 cm H₂O, and nonsignificant for 6 vs 8 cm H₂O.

Vₜ = tidal volume
f = breathing frequency
Pspell = end-tidal carbon dioxide pressure
τ = time constant of relaxation of the respiratory muscles

We elected to use the ventilation efficiency index in our study because it is a composite index of ventilation that incorporates information on both the input (breathing frequency and pressures) and the output (CO₂) of the process of ventilation being an ideal index to describe ventilation efficiency. In our study, we reported values of ventilation efficiency index that were relatively higher than in previously published studies; this was due to the relatively lower spontaneously generated inspiratory pressure in our study, which might be explained by the dampening of the pressure in the endotracheal tube. Furthermore, to avoid excessive arterial blood sampling over a very short period of time, we used P ET CO₂ and not arterial CO₂ values. When compared with term-born infants, premature infants have an increased anatomic dead space, so P ET CO₂ is very likely to be lower than arterial CO₂. We studied the range of CPAP levels in each infant, so factors like the increased dead space and relatively increased ventilation efficiency index did not influence the validity of our conclusions.

We also elected to use the respiratory muscle time constant of relaxation to assess respiratory muscle function. The airway pressure decay is a proxy for the rate of relaxation of the respiratory muscles and a well-described measure of respiratory muscle fatigue. τ has been used to successfully predict the outcome of extubation in studies of adults on ventilation.

Contrary to the aforementioned studies, the Vₜ in our study was not significantly higher at increasing levels of CPAP. Those differences might be explained by population and methodologic differences: Our infants were well enough to be considered for extubation and were studied while intubated. Intubation might have impacted on the mechanics of the respiratory system by bypassing the contribution of the upper airways and by imposing an added resistance, which corresponds to the endotracheal tube.

Invasive or more complex methods, such as the estimation of the diaphragmatic tension-time index, are not feasible.
or diaphragmatic electromyography, would focus on diaphragmatic function rather than on all respiratory muscles. The advantage of our approach was that qualitative analysis of the pressure waveform and the corresponding time constant of respiratory muscle relaxation can be incorporated into ventilator software and displayed in real time, which thus aids clinical decision-making on the optimal level of CPAP at the bedside.

The findings of our study are physiologically plausible. The sigmoid nature of the compliance curve of the respiratory system would dictate that the work of breathing was increased in both ends of the pressure spectrum. Achieving a set VT at relatively low pressures is energy inefficient because of atelectasis and lung de-recruitment at low pressures. Similarly, at relatively high pressures, the work of breathing would also increase because of the effect of hyperinflation on diaphragmatic contractility, which thus left an optimal ventilation zone in-between these two extremes. Our study highlighted that the majority of convalescent prematurely born infants would be in this zone at a distending pressure of 6 cm H2O.

Recent animal studies in ARDS furthered our understanding of how a higher level of CPAP could be beneficial to respiratory function. A higher PEEP minimized dependent lung injury via lung stretch and stretch in adults with severe ARDS and animal models of ARDS, whereas a PEEP of 5 cm H2O but not a PEEP of 2 cm H2O reduced lung damage and inflammatory markers.

Our study had strengths and some limitations. To our knowledge, this was the first study to describe respiratory muscle function changes at different levels of CPAP in premature infants on ventilation. This study was conducted in infants on ventilation and had the obvious methodologic advantage of accurate pressure and CO2 measurements. Previous plethysmographic studies could not have measured and analyzed the pressure waveform that provides the surrogate for the assessment of the respiratory muscles. Furthermore, measurement of CO2, and thus ventilation efficiency, cannot be undertaken in infants who were not on ventilation without the application of a face mask, which, by adding a significant dead space, might considerably impact the accuracy of the measurements and even on the breathing pattern. In our study, we included a population that was studied at varying ages and FIO2 requirements. A more homogeneous population might have decreased the variation in our outcome measures, but we believe that our population mirrored the corresponding variation encountered in everyday clinical practice.

We acknowledge as a limitation that this study was conducted on stable infants on ventilation and our results might not be directly translatable to the level of CPAP that is required when given in a noninvasive manner or in prematurely born infants studied during the acute phase of respiratory distress syndrome. Because this was a crossover study of the same infants, however, the relationship of unloading the respiratory muscles and increasing the ventilation efficiency with increasing levels of CPAP was valid. Previous studies question the validity of tidal capnographic measurements in premature infants due to technical limitations that arise from the high proportion of instrumental dead space to VT and the breathing pattern of premature infants, which involves high rates and, commonly, the absence of an alveolar plateau phase. In our study, however, we used a capnograph with the lowest available dead space, so this error has been minimized. Also, because the same methodology was used to measure PETCO2, the relative change in PETCO2 at different levels of CPAP would also be valid.

Conclusions

We demonstrated that increasing the distending pressures of CPAP from 4 to 6 cm H2O was associated with enhanced ventilation efficiency and respiratory muscle function, but there was no further benefit from exceeding a level of 6 cm H2O.

ACKNOWLEDGMENTS

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REFERENCES

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